

1                   **Radiation Biodosimetry Devices**  
2                   **Draft Guidance for Industry and**  
3                   **Food and Drug Administration Staff**

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5                   ***DRAFT GUIDANCE***

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10  
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14                   Division of Dockets Management (HFA-305), Food and Drug Administration, 5630 Fishers Lane,  
15                   rm. 1061, Rockville, MD 20852. Identify all comments with the docket number listed in the  
16                   notice of availability that publishes in the *Federal Register*.

17  
18                   For questions about this document, contact the Division of Molecular Genetics and Pathology at  
19                   301-796-6179 or Jennifer Dickey at 301-796-5028 or via email at [Jennifer.Dickey@fda.hhs.gov](mailto:Jennifer.Dickey@fda.hhs.gov).



U.S. Department of Health and Human Services  
Food and Drug Administration  
Center for Devices and Radiological Health

Office of *In Vitro* Diagnostics and Radiological Health  
Division of Molecular Genetics and Pathology Devices

## **Preface**

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# Radiation Biodosimetry Devices

## Draft Guidance for Industry and Food and Drug Administration Staff

*This draft guidance, when finalized, will represent the Food and Drug Administration's (FDA's) current thinking on this topic. It does not create or confer any rights for or on any person and does not operate to bind FDA or the public. You can use an alternative approach if the approach satisfies the requirements of the applicable statutes and regulations. If you want to discuss an alternative approach, contact the FDA staff responsible for implementing this guidance. If you cannot identify the appropriate FDA staff, call the appropriate number listed on the title page of this guidance.*

### I. Introduction

FDA has developed this draft guidance to facilitate study designs to establish the analytical and clinical performance characteristics of radiation biodosimetry medical countermeasure devices. Radiation biodosimetry countermeasure devices are devices used for the purpose of reconstructing the ionizing radiation dose received by individuals or populations using physiological, chemical or biological markers of exposure found in humans. Radiation biodosimetry technologies may be used at various stages during triage and treatment after the exposure of a population to ionizing radiation as a result of intentional harm or as an unintended consequence of a disaster. Devices may be designed to give quantitative outputs or qualitative information around a clinical decision making cut-point. Likewise, devices may be designed for use in field triage settings, at patient bedsides, or in Clinical Laboratory Improvement Amendments of 1988 (CLIA) certified clinical laboratories. FDA considered both high-throughput and single-use devices in developing this draft guidance document.

This draft guidance document does not provide specific study designs; it describes design principles for studies that may be used to establish a reasonable assurance of the safety and effectiveness of radiation biodosimetry devices. Sponsors should develop a validation plan to establish the analytical, pre-clinical, and clinical performance characteristics in order to substantiate the claims in the device intended use statement, and discuss this plan with the FDA prior to beginning studies.

Throughout this guidance document, the terms “we,” “us” and “our” refer to FDA staff from CDRH. “You” and “your” refers to the applicant or sponsor.

FDA's guidance documents, including this draft guidance, do not establish legally enforceable responsibilities. Instead, guidances describe the Agency's current thinking on a

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127 topic and should be viewed only as recommendations, unless specific regulatory or statutory  
128 requirements are cited. The use of the word *should* in Agency guidance means that  
129 something is suggested or recommended, but not required.  
130

## 131 II. Background

132  
133 A radiological event, for instance from use of an improvised nuclear device or radiological  
134 dispersal device or from a natural disaster, could potentially expose thousands of individuals  
135 to high levels of radiation that would require immediate assessment and medical intervention.  
136 A coordinated medical response including triage and treatment would be important to  
137 mitigate harm resulting from the unintended exposure of individuals to ionizing radiation.  
138 Radiation biodosimetry tools would be a critical component of such a response.  
139 Biodosimetry is a surrogate for knowledge of the absolute dose delivered to an individual. It  
140 allows for the assessment of the likelihood of a patient developing acute radiation syndrome  
141 (ARS) and to develop an appropriate treatment plan for the patient.

142 Most radiation biodosimetry devices are *in vitro* diagnostic devices (IVDs), as defined in 21  
143 CFR 809.3(a).<sup>1</sup> However, a wide array of technologies may be employed to assess biological  
144 responses to radiation. Methodologies amenable to radiation biodosimetry devices could  
145 include nucleic acid based devices that utilize technologies such as polymerase chain reaction  
146 (PCR) or microarrays, devices designed to detect changes in protein expression using  
147 technology such as enzyme-linked immunosorbent assays (ELISA) or flow cytometry, and  
148 devices designed to detect other biological signals induced by exposure to radiation.  
149

150 Sponsors who intend to market radiation biodosimetry devices must, in addition to other  
151 applicable requirements, conform to the general controls of the Federal Food, Drug, and  
152 Cosmetic Act (FD&C Act), and obtain premarket clearance or approval prior to marketing  
153 their devices. When finalized, this draft guidance document will represent our current  
154 thinking regarding the recommended design of studies to demonstrate a reasonable assurance  
155 of the safety and effectiveness of radiation biodosimetry devices for unintended exposures to  
156 radiation. We consider these recommended studies to be relevant for premarket notifications  
157 (e.g., 510(k) submissions or premarket approval applications (PMAs) that may be required  
158 for a particular device). General information about 510(k) submissions and PMAs are  
159 outlined in the following guidances:

- 160
- 161 • “Format for Traditional and Abbreviated 510(k)s”  
162 ([http://www.fda.gov/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocu  
163 ments/ucm084365.htm](http://www.fda.gov/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/ucm084365.htm))

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<sup>1</sup> *In vitro diagnostic products* are those reagents, instruments, and systems intended for use in the diagnosis of disease or other conditions, including a determination of the state of health, in order to cure, mitigate, treat, or prevent disease or its sequelae. Such products are intended for use in the collection, preparation, and examination of specimens taken from the human body. These products are devices as defined in section 201(h) of the Federal Food, Drug, and Cosmetic Act (the act), and may also be biological products subject to section 351 of the Public Health Service Act.

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- 164 • “Acceptance and Filing Reviews for Premarket Approval Applications (PMAs)”  
165 (<http://www.fda.gov/downloads/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/UCM313368.pdf>)  
166  
167

168 Further information on device regulation can be found at “Device Advice”  
169 (<http://www.fda.gov/MedicalDevices/DeviceRegulationandGuidance/default.htm>).  
170

171 FDA recognizes that biodosimetry device sponsors face unique challenges in attempting to  
172 meet premarket clearance or approval requirements for their devices. For example, ethical  
173 considerations limit the availability of appropriate clinical samples for biodosimetry device  
174 performance studies, leading to the expected use of animal models as surrogates for clinical  
175 validation purposes. As such, study designs that are not typically recommended for other  
176 IVD submissions may be appropriate for radiation biodosimetry devices. The intent of this  
177 guidance document is to provide clarity to both industry and FDA staff on the performance  
178 data that should be included in a premarket submission in order to help sponsors design  
179 studies, and to facilitate our review process. Due to the device’s novelty, the pre-submission  
180 process is an encouraged component of any radiation biodosimetry device development plan.  
181 Information on the pre-submission process can be found in the guidance document entitled  
182 “Requests for Feedback on Medical Device Submissions: The Pre-Submission Program and  
183 Meetings with Food and Drug Administration Staff”  
184 (<http://www.fda.gov/downloads/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/UCM311176.pdf>).  
185  
186

### 187 **III. Scope**

188  
189 This draft guidance only applies to validation of biodosimetry devices intended to be used to  
190 assess exposure in non-therapeutic or accidental scenarios (e.g., a deliberate attack, such as  
191 use of an improvised nuclear device, or a natural disaster). This guidance neither applies to  
192 devices that assess deliberate radiation dosing that may occur in the course of medical  
193 treatment nor to devices that measure effects from long term exposure. In addition,  
194 dosimeters, which are devices that detect radiation exposure on a physical substrate rather  
195 than through a biological response and are worn by people who might be exposed to  
196 radiation during the course of their normal work (such as film badges), are not addressed in  
197 this guidance document. Finally, biological assays that might be used to detect the presence  
198 of ingested radioisotopes in sputum or urine are not considered in this guidance document.  
199

### 200 **IV. Policy**

#### 201 **A. Benefit-Risk Analysis**

202  
203  
204 A source of significant risk to patient health associated with radiation biodosimetry devices is  
205 when a failure of the device to perform as indicated leads to either deficient or inaccurate  
206 results or the incorrect interpretation of these results. Inappropriate or incorrect use of  
207 radiation biodosimetry devices may be an additional risk. These potential risks may then

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208 lead to incorrect patient management decisions. For instance, a false positive result or  
209 overestimation of exposure in an emergency scenario with adequate resources could lead to  
210 unnecessary or inappropriate treatment for ARS. Alternatively, an overestimation of  
211 exposure in a resource poor mass exposure scenario may result in the patient being  
212 inappropriately placed in an expectant category and given only palliative care when treatment  
213 could be life-saving. Likewise, from a public health standpoint, a false positive result in a  
214 resource poor response area could lead to a misallocation of resources. However, a false  
215 negative result or underestimation of exposure could lead to failure to provide treatment or  
216 incorrect patient management which may be lethal. Thus it is essential to appropriately  
217 balance the benefits and risks of false negative and false positive results.

218

219 Current laboratory methods for determining absorbed radiation doses utilize cell based assays  
220 that are accurate, but take several days to complete. Therefore, part of evaluating the  
221 benefit/risk considerations for new radiation biodosimetry systems will be evaluating  
222 performance differences along with the overall time to result or throughput of the system  
223 (e.g., decreased accuracy may be acceptable for a device that provides a more rapid result in  
224 the context of triage). The guidance document entitled “Factors to Consider When Making  
225 Benefit-Risk Determinations in Medical Device Premarket Approvals and De Novo  
226 Classifications”

227 ([http://www.fda.gov/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/u](http://www.fda.gov/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/ucm267829.htm)  
228 [cm267829.htm](http://www.fda.gov/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/ucm267829.htm)) provides information on FDA benefit-risk determinations. Premarket  
229 submissions should include a discussion of the potential benefits and risks associated with  
230 the device in light of the biological radiation response pathway that is being assessed, the  
231 analytical strengths and weaknesses of the technology, and the clinical information that is  
232 available demonstrating device effectiveness.

233

### **B. Device Description and Specifying the Intended Use**

234

235  
236 All components of your radiation biodosimeter system necessary to achieve the claimed  
237 functionality in the intended use statement should be listed in the device description.

238

239 The intended use statement should specify 1) the nature of the analyte (e.g., RNA, DNA, or  
240 protein), 2) specimen types in which testing may be performed (e.g., blood, urine, or saliva),  
241 and 3) the specific population(s) for which the test is intended (e.g., pediatrics, general  
242 population).

243

244 The intended use statement should also explain whether the test is qualitative or quantitative  
245 and include any specific conditions of use. The intended use statement of most radiation  
246 biodosimetry devices should also explicitly advise that results need to be considered in  
247 combination with other appropriate clinical signs and symptoms as well as radiation dispersal  
248 monitoring.

249

250 Additional specific elements that should be considered for radiation biodosimetry devices  
251 include the following:

252



253 **1. The stage of response for which your device is intended**

254

255 Biodosimetry devices may be designed for preliminary triage during a mass exposure event.  
256 For these types of devices, the intended use should specify the throughput capabilities, and  
257 time to result of the device and the decision making cut-points assessed. Alternatively,  
258 biodosimetry devices may be designed for dose level confirmation and medical management  
259 at later stages of a mass exposure scenario or in situations where only a small number of  
260 people need to be assessed. For these types of devices, the assay analytical range and  
261 specific clinical indicators of health status should be part of the intended use statement.

262

263 **2. Appropriate time-frames for testing**

264

265 Because many common biomarkers of radiation exposure display defined kinetics, during  
266 which they become detectable, remain stable, and then disappear from the matrix being  
267 examined, it is important to specify the time-frame in which the device is designed to  
268 function, beginning from time of exposure. This should include both the beginning and end  
269 of the acceptable testing window (e.g., from 30 minutes to 48 hours post-exposure).

270

271 **3. Assay limitations**

272

273 Validation of radiation biodosimetry devices may be incomplete due to a lack of samples  
274 from the intended use population. Therefore, limitation statements may be needed to  
275 minimize risk of over-reliance on biodosimeter results when the real world situation in which  
276 the device is being used does not mirror the scenarios tested. For instance, if validation  
277 testing was only performed on certain populations (e.g., not tested in pediatrics), for specific  
278 radiation types (e.g., exposure to gamma source only), or on specimens or subjects exposed  
279 to limited doses and dose rates that may not reflect the final situation of use, these limitations  
280 should be captured in the labeling. Other situations that may cause inaccurate biodosimeter  
281 results (e.g., combined injury such as radiation plus physical trauma) should be taken into  
282 account when drafting an appropriate intended use statement. However, labeling limitations  
283 cannot generally be relied upon to justify missing validation studies using the intended use  
284 population. You should make every attempt to capture the intended use population. If you  
285 determine that you are unable to perform validation using the intended use population, you  
286 should provide a justification along with a detailed description of the due diligence activities  
287 you performed to support your validation approach.

288

289 **C. Establishing Performance Characteristics – Analytical**  
290 **Validation Studies**

291

292 The most significant benefit that radiation biodosimetry has over standard dosimetry is that  
293 biodosimetry takes into account the natural patient biological variability in radiation  
294 response, though dosimetry tools may provide a more accurate representation of the actual  
295 radiation dose delivered. For example, while a standard dosimeter may give an accurate  
296 representation of dose, standard dosimetry devices will be unable to differentiate a patient

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297 who is radiation sensitive (presumably needing a higher level of medical intervention) from a  
298 patient who is radiation resistant. As such, the development of radiation biodosimetry  
299 techniques will be a powerful tool in personalizing therapeutic responses to radiation  
300 exposure, representing a significant benefit to public health. However, because biological  
301 response to a radiation dose is measured by biodosimetry, the measurement is confounded by  
302 patient-to-patient variation in radiation resistance making simple dose/response correlations  
303 difficult. As such, a well-documented explanation of the relevant biological pathways should  
304 be provided to FDA in order to justify a lack of correlation to an accuracy standard  
305 attributable to natural biological response. Such information can be obtained through peer-  
306 reviewed literature as well as bench testing. Well-controlled analytical studies should be  
307 provided to FDA to establish device performance across the entire analytical range of the  
308 device in a defined sample subset. This analytical performance information will be critical to  
309 substantiate intended use claims of a radiation biodosimetry device.

310

311 As discussed in section II, radiation biodosimetry devices generally will be IVDs.  
312 Accordingly premarket submissions will generally be reviewed by the Office of *In Vitro*  
313 Diagnostics and Radiological Health (OIR). This section provides specific recommendations  
314 to facilitate planning your validation studies. You are encouraged to consider relevant  
315 guidance documents for general information on what to include in submissions and the types  
316 of studies that may be expected. The following two documents may be useful in preparing  
317 premarket submissions:

318

- 319 • “In Vitro Diagnostic (IVD) Device Studies – Frequently Asked Questions”  
320 (<http://www.fda.gov/medicaldevices/deviceregulationandguidance/guidancedocument/s/ucm078309.htm>)  
321
- 322 • “eCopy Program for Medical Device Submissions”  
323 (<http://www.fda.gov/downloads/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/UCM313794.pdf>)  
324

325

326 Additionally, it is beyond the scope of this document to consider the broad range of  
327 analytical characteristics specific to each of the many and varied technologies that may be  
328 employed to develop radiation biodosimeters. Therefore, you are encouraged to examine  
329 guidance documents that might be applicable to the type of technology your device employs  
330 to identify the types of analytical characteristics that might be appropriate to demonstrate for  
331 your device. For example, if a biodosimetry instrument utilizes a genetic test for heritable  
332 markers, you might consider consulting the “Guidance on Pharmacogenetic Tests and  
333 Genetic Tests for Heritable Markers”  
334 (<http://www.fda.gov/downloads/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/ucm071075.pdf>) to identify the types of analytical characteristics that might be  
335 appropriate to demonstrate for your device.  
336

337

338 Finally, appropriate standards documents drafted by the Clinical and Laboratory Standards  
339 Institute (CLSI) are additional helpful resources that might provide details on specific  
340 analytical performance testing appropriate for your device. Specific standards documents  
341 which might be applicable will be referenced throughout this section. A list of FDA

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342 recognized standards can be found at the following website:  
343 <http://www.accessdata.fda.gov/scripts/cdrh/cfdocs/cfStandards/search.cfm>.

344

### 345 **1. Sample availability**

346

347 We recognize the difficulty in acquiring appropriate clinical samples for use during device  
348 validation. Two possible sources of clinical samples include site-limited radiation therapy  
349 patients and total body irradiation (TBI) patients. However, these specimens may be difficult  
350 to obtain in sufficient amounts. Another challenge with these sources is that the therapeutic  
351 protocol restricts the dose exposures available (only low dose fractionated exposures may be  
352 readily obtained). In the absence of sufficient or appropriate clinical samples, contrived  
353 samples may be used to supplement clinical samples for analytical performance testing, but  
354 only as a supplement to, and not as a substitute for, clinical samples.

355

356 Samples may be contrived by *ex vivo* irradiation of the appropriate matrix, spiking the  
357 analyte of interest into the appropriate matrix, or through the use of animal-derived  
358 specimens, as appropriate. In some instances, control material may be used for the purposes  
359 of analytical performance testing. Premarket submissions should include a scientific  
360 justification for contrived sample utilization, a description of how contrived samples were  
361 generated and validated for testing, and a description of how the results obtained translate to  
362 the clinical setting. You are encouraged to discuss the most appropriate sample type for  
363 testing with FDA prior to designing your analytical validation studies. The proportion of  
364 samples that may be contrived for analytical validation testing will depend on both the  
365 technological characteristics of the device and the abundance of appropriate samples. You  
366 should be thorough in attempting to obtain and use appropriate clinical samples to  
367 demonstrate performance.

368

### 369 **2. Specimen collection and handling**

370

371 The quality and quantity of an extracted analyte can be affected by multiple factors such as  
372 specimen source, collection method, and handling (e.g., transport, storage time, and  
373 temperature). Therefore, premarket submissions should include performance validation data  
374 to establish that the specimen collection and transport system employed by the device  
375 provides an adequate and appropriate yield of the analyte being detected by the assay (e.g.,  
376 DNA or RNA from blood or tissue). Testing should also demonstrate that the device  
377 maintains acceptable performance under all the various specimen handling conditions  
378 claimed in the product labeling.

379

380 Specimen stability should be addressed in the radiation biodosimetry premarket submission.  
381 However, we recognize there may be different analytical and clinical performance needs  
382 depending on whether the device is intended for initial triage in a field setting, for radiation  
383 exposure confirmation, or for dose refinement in a clinical laboratory setting.

384

385 For example, if the device is intended to be used in a field triage environment, CDRH would  
386 evaluate whether the device is both sufficiently robust to withstand environmental impacts

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387 and appropriately user friendly for use by the intended user. Therefore, for biodosimetry  
388 devices intended for field triage use, performance testing should include performance testing  
389 to demonstrate the robustness of the device, and where relevant, performance testing to  
390 demonstrate the device’s specimen collection and transport performance characteristics. By  
391 contrast, performance evaluation of devices intended for dose refinement may focus more on  
392 performance testing to demonstrate the device’s measurement precision performance  
393 characteristics. In either case, specimen shipping stability performance testing will be critical  
394 if the testing is intended to take place far from where the patient samples are obtained. The  
395 acceptance criteria for all specimen stability parameters should be clearly indicated and  
396 justified in terms of the intended use environment as indicated in the labeling.

### **3. Accuracy**

397  
398  
399  
400 In order to demonstrate analytical accuracy, the device’s measurement of the biological  
401 response to radiation is compared to the physical calculated dose delivered. Therefore, the  
402 accuracy of the delivered dose is crucial, and the protocol for designing proper telemetry  
403 should be included in all study protocols. As discussed above, we expect that because the  
404 biodosimetry output will be confounded by the biological response to radiation, there will be  
405 inter-individual variations which may complicate the correlation of the output to the accuracy  
406 standard.

407  
408 In the case of human clinical samples, since the exposure rates and overall dose will be  
409 dictated by the therapeutic protocol, there will be no need to justify the doses and dose rates  
410 used. Nevertheless, submissions should include information on the radiation source, dose  
411 delivered, dose rate, and the time intervals at which device testing was performed. When  
412 animal studies are being used to supplement human clinical samples, a scientific justification  
413 for the dose rates and doses delivered should be included in the submission, in addition to  
414 information on the radiation source, dose delivered, dose rate and time intervals. Animal  
415 studies should be designed to “bridge” between animal and human biological response with  
416 the human radiation protocol duplicated in the animal study, while other animal studies  
417 should supply information on test performance using doses/dose rates that cannot be ethically  
418 obtained in human clinical studies.

419  
420 Statistical analysis plans including acceptance criteria should be developed around accuracy  
421 studies, and be appropriate for the device output (qualitative or quantitative). Please refer to  
422 Appendix A in section V of this document for more information on statistical considerations  
423 for study designs. All accuracy studies should be designed to demonstrate device  
424 performance at the relevant clinical decision making points relevant to the intended use of  
425 your device (i.e., triage or medical management) and contain pre-specified success criteria.  
426 The rationale for your acceptance criteria should be provided and clinically justified.

427  
428 The reference method used to evaluate accuracy of the biodosimetry device will depend on  
429 your device’s intended use. For example, if the device is intended for use in both triage and  
430 confirmation, a reference method currently used for small-scale radiation exposures, such as  
431 the dicentric chromosome assay, may be appropriate. However, chromosome-based assays

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432 may not be an appropriate comparator for devices designed for triage due to the time needed  
433 to perform this reference method.

434

### 435 **4. Analytical range**

436

437 If a radiation biodosimetry device reports numerical (quantitative) results, submissions  
438 should include studies establishing the analytical range of your device. Analytical range  
439 studies should be designed to substantiate Limit of Detection (LoD), Limit of Blank (LoB),  
440 Limit of Quantitation (LoQ) and the linear range claims of the assay. The clinically relevant  
441 range of exposure is 0-10 Gy and we recommend developing test protocols to demonstrate  
442 the limitations of your assay outside the reportable range (both above and below). For  
443 instance, if high exposure levels can cause the assay to incorrectly report lower values (i.e.,  
444 the hook effect), then the limitations section of the labeling would include this information.  
445 Please refer to the CLSI document EP6-A, “Evaluation of the Linearity of Quantitative  
446 Measurement Procedures: A Statistical Approach,” and EP17-A2, “Protocols for  
447 Determination of Limits of Detection and Limits of Quantitation” to assist in the design of  
448 such studies. Samples around critical decision making cut-points should also be included in  
449 analytical range validation studies.

450

### 451 **5. Interference**

452

453 Interfering substances may confound assay outputs. As such, radiation biodosimetry device  
454 submissions should include the results of appropriate interference studies (see CLSI  
455 Document EP7-A2 “Interference Testing in Clinical Chemistry”). Interference studies may  
456 be specific to the matrix being examined. For example, if the assay uses blood, interference  
457 from hemoglobin, bilirubin, and lipids should be examined to mimic grossly hemolytic,  
458 icteric and lipemic samples. Likewise common drugs known or expected to interfere, or  
459 drugs that are expected to be administered in a mass radiation exposure scenario, should be  
460 tested for assay interference. See the document entitled “Planning Guidance for Response to  
461 a Nuclear Detonation” (<http://www.remm.nlm.gov/PlanningGuidanceNuclearDetonation.pdf>)  
462 for more information on the Federal government response plans for radiation disaster  
463 scenarios and the applicable drugs and treatments that will be recommended in such a  
464 scenario. (Note this website is not controlled by FDA. The content of the website was last  
465 verified on December 18, 2014.) In addition, you should consider how biological responses  
466 may interfere with your assay and develop corresponding risk mitigations necessary to  
467 provide a reasonable assurance of safety and effectiveness (e.g., to limit the interfering  
468 effects of the underlying biological response). This information may be appropriate to  
469 include in the warnings and limitations section in the labeling. Ultimately the decision of  
470 what compounds to test for assay interference should be based on applying scientific  
471 reasoning to the technological characteristics of your device and the major biological  
472 pathways being interrogated. For instance, if a radiation biodosimeter incorporates  
473 expression profiles from a pro-inflammatory pathway, interference from anti-inflammatory  
474 drugs should be examined and assay effectiveness should be tested in normal volunteers with  
475 possible confounding diseases such as arthritis and other inflammatory conditions.

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476 Alternatively, animal models may be used to evaluate these potential confounders (see  
477 section IV(D) below).

478

479

### **6. Other analytical testing protocols**

480

481 Analytical testing protocols, in addition to those mentioned specifically above, should be  
482 included in radiation biodosimetry submissions as applicable given the intended use, output,  
483 and technology. Reproducibility generally should be demonstrated at a minimum of three  
484 sites (of which at least one should be in the United States) and submissions should include an  
485 analysis of site-to-site, operator-to-operator, instrument-to-instrument, and kit lot-to-kit lot  
486 reproducibility as applicable. The limits of detection, quantitation, and blank, as relevant,  
487 may be demonstrated in a separate study or in combination with the analytical range study.  
488 The stability of kit reagents should be performed in real-time for product expiry dating, and  
489 should also be examined in shipping simulation studies. As noted above, studies to support  
490 technology-specific validation and special controls may apply, such as for molecular assays.

491

492 In addition to CLSI documents indicated elsewhere in this document, the following may be  
493 useful in understanding how such analytical performance studies are typically designed:

494

- 495 • EP5-A2, “Evaluation of Precision Performance of Quantitative Measurement  
Methods”
- 496 • EP9-A2, “Method Comparison and Bias Estimation Using Patient Samples”
- 497 • EP12-P, “User Protocol for Evaluation of Qualitative Test Performance”
- 498 • EP17-A2, “Protocols for Determination of Limits of Detection and Limits of  
499 Quantitation”
- 500 • EP25-A, “Evaluation of Stability of *In Vitro* Diagnostic Reagents”

501

502

### **7. Controls and calibrators**

503

504 The design of radiation biodosimetry devices should incorporate the use of on-board or  
505 external controls as appropriate. Any recommended Quality Control (QC) procedures and  
506 acceptance criteria used during the analytical and clinical validation of your device should be  
507 included in the instructions for use. A description of the control material and its  
508 recommended use should be submitted along with the assay for premarket clearance or  
509 approval. Information that should be provided in the premarket submission includes control  
510 performance, value assignment, and reagent stability as outlined in guidance entitled  
511 “Assayed and Unassayed Quality Control Material”

512 (<http://www.fda.gov/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/ucm079179.htm>).

513 Similarly, if external calibrators are required for the assay system, they  
514 should also be submitted with the assay. You are encouraged to consult the guidance entitled  
515 “Abbreviated 510(k) Submissions for In Vitro Diagnostic Calibrators”

516 (<http://www.fda.gov/downloads/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/ucm092801.pdf>).

517

518



519 **8. Instrumentation and software**

520

521 If your radiation biodosimetry device utilizes software, you should submit the information  
522 listed in the guidances entitled “Guidance for the Content of Premarket Submissions for  
523 Software Contained in Medical Devices”

524 (<http://www.fda.gov/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/ucm089543.htm>) (“Software Premarket Submissions Guidance” for the duration of this

525 document) and “Guidance for Off-the-Shelf Software Use in Medical Devices”

526 (<http://www.fda.gov/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/ucm073778.htm>).

527 The information you should submit is determined by the “level of concern,”  
528 which is related to the risks associated with software failure, as explained in the Software  
529 Premarket Submissions Guidance.  
530

531

532 **D. Establishing Performance Characteristics – Animal**  
533 **Studies as Surrogates for Clinical Validation**

534

535 Traditionally, animal data are not used in IVD submissions. IVD sponsors are expected to  
536 obtain specimens from the intended use population either through prospective collection  
537 from a trial or to use properly archived surplus (excess) specimens to demonstrate test  
538 performance when prospective studies are not feasible. However, in the case of radiation  
539 biodosimetry devices, we acknowledge that appropriate human specimens may not be  
540 available. Therefore, under the following conditions it may be appropriate to use animal  
541 model data to supplement human clinical samples to demonstrate device performance:

- 542
- 543 • The analyte(s) being detected is not stable in archived specimens;
  - 544 • A diligent search of available specimen banks has failed to yield adequate  
545 samples for testing; or
  - 546 • A prospective trial is either unethical, or prospective trials that may be ethically  
547 performed will not yield a sample set adequate to demonstrate assay performance  
548 over the analytical range of the device.

548

549 **1. Defining an appropriate animal model**

550

551 If animal model data is included in a biodosimetry device premarket submission, the  
552 submission should also include an appropriate justification for the animal model or models  
553 chosen. You should provide evidence that the model is an appropriate substitute for human  
554 specimens. In particular, establishing that there is high homology in the analyte(s) being  
555 assessed and that the animal model displays similar responses to radiation exposure in the  
556 biological pathways being interrogated is important. While rodent models may be  
557 appropriate for early proof of concept studies, they are not typically adequate for  
558 demonstrations of device effectiveness. Primate or porcine models, in which radiation  
559 biological response pathways are well understood, may be the best option for effectiveness  
560 studies. You should ensure that an equal distribution of genders is included in pre-clinical  
561 testing and consider including animals at various age ranges (e.g., juvenile, adult, elderly) so

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562 age and gender-related differences in radiation response can be assessed for the analytes  
563 included in the biodosimetry testing.

564

565 As stated above, for biodosimetry device effectiveness studies, animal models should  
566 supplement and not be a substitute for human clinical samples. Therefore, multiple animal  
567 models generally are not required to demonstrate the biodosimeter's effectiveness. However,  
568 multiple animal models may be necessary when a single appropriate animal model cannot be  
569 identified for all analytes being assessed by the device.

570

571 Please note that all device effectiveness studies using animal models must comply with good  
572 laboratory practice for nonclinical laboratory studies regulations as described in 21 CFR Part  
573 58, including 21 CFR 58.90. Further, FDA recommends that you follow the Animal Welfare  
574 Act, PHS policy, and their applicable regulations and statutes. FDA believes that following  
575 these regulations enhances the opportunity and intensity of observations and can potentially  
576 result in other useful findings for the investigators (see Ref. 1-4).

577

### 578 **2. Effect of “supportive care” on device output**

579

580 In some cases, animal housing and supportive care conditions might influence radiation  
581 biodosimetry assay results. For instance, analyte expression might be influenced by  
582 differences in diet or lifestyle patterns of laboratory animals as opposed to that of the general  
583 human population. You should make an attempt to address the effect of confounding factors  
584 that may be associated with aspects of animal care that will not be reflective of the intended  
585 use population. Additionally, to avoid variability caused by changes in radiation response  
586 due to circadian rhythm patterns, you should deliver radiation at the same time of day (e.g.,  
587 a.m. vs. p.m.) to all animal models in pre-clinical testing.

588

589 You also may want to consider providing animal models with the same supportive care that  
590 is expected to be provided to people in a radiation mass exposure scenario, such as antibiotics  
591 and fluids, to determine if these types of medical interventions alter the biological responses  
592 being assessed by biodosimetry. See the document entitled “Planning Guidance for  
593 Response to a Nuclear Detonation”

594 (<http://www.remm.nlm.gov/PlanningGuidanceNuclearDetonation.pdf>) for more information  
595 (Note this website is not controlled by FDA. The content of the website was last verified on  
596 December 18, 2014). For example, if neutrophil numbers are part of a biodosimetry  
597 algorithm, it should be understood how G-CSF treatments affect resulting exposure level  
598 estimations. This information may be critical to ensuring appropriate labeling is provided for  
599 the assay.

600

### 601 **3. Bridging animal data to human data**

602

603 When animal model data are necessary to demonstrate the effectiveness of a radiation  
604 biodosimeter across the reportable analytical assay range, then two types of studies should be  
605 provided. First, a set of experiments should be designed to bridge between the animal results  
606 and the available human clinical information. For instance, if available human samples were



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607 derived from whole body exposure delivered in 2 Gy fractions over the course of a week,  
608 then an animal study should be performed to mirror this exposure pattern to demonstrate how  
609 animal results and human data are reflective of each other. Once an appropriate  
610 demonstration has shown that animal results can be bridged to human clinical experience,  
611 then studies in animals may be performed to address device performance at radiation doses,  
612 dose-rates, time-courses, and sources that cannot be examined in human clinical studies.

613

614 Animal studies may also be used to address situations that may not be easily addressed using  
615 human clinical studies. For instance, you should consider testing with commonly used drugs  
616 such as anticholesterol, antihypertension, diabetic drugs, and other common drugs if there is  
617 evidence to suggest that they may interfere with the analyte being evaluated (e.g., a particular  
618 metabolic pathway CYP450, growth factors). Other situations that may confound assay  
619 results such as combined injury can also be examined in pre-clinical models.

620

621 Animal studies should be designed to use the fewest possible animals to demonstrate  
622 statistical significance. Because these studies will be critical to demonstrate the performance  
623 of a radiation biodosimeter and because alternative study designs will be needed to minimize  
624 animal numbers, it is encouraged that study protocols be submitted to us prior to the onset of  
625 testing in order to gain Agency concurrence on study parameters and statistical analysis  
626 plans. Please refer to the appendix in section V of this document for more information on  
627 statistical considerations for radiation biodosimetry study designs.

628

### 629 **E. Establishing Performance Characteristics – Clinical** 630 **Validation Studies with Human Samples**

631

632 FDA expects that radiation biodosimeter safety and effectiveness will be established in a  
633 clinical study that contains appropriate human samples. As discussed above, non-clinical  
634 models may be used to supplement human clinical data by providing data on doses, dose  
635 rates, and radiation sources that cannot be ethically obtained in a human clinical study.  
636 However, manufacturers should strive to perform validation studies using the intended use  
637 population of the device. These pivotal studies should be designed with an appropriate  
638 statistical analysis plan in place with pre-defined acceptance criteria. You are encouraged to  
639 refer to Appendix A in section V of this document and the guidance entitled “Statistical  
640 Guidance on Reporting Results from Studies Evaluating Diagnostic Tests”  
641 (<http://www.fda.gov/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/ucm071148.htm>)  
642 for more information.

643

#### 644 **1. Prospective clinical studies**

645

646 Samples may be collected prospectively for biodosimeter clinical testing in the context of  
647 radiation exposure for therapeutic purposes. For instance, patients may consent to provide  
648 blood, tissue, or other relevant samples during the course of standard radiation therapy or in  
649 the context of radiation therapy clinical trials. Information should be captured on the dose,  
650 dose rate, and source of exposure for all patients included in prospective testing. In addition,

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651 basic demographic information should be collected, including patient age, gender, and race.  
652 Whenever possible, information on the patient’s clinical condition and medications should  
653 also be collected.

654

655 Prospective IVD clinical studies that do not require an invasive sampling procedure and for  
656 which the test results are not used to support patient management are generally considered to  
657 meet the requirements under 21 CFR 812.2(c)(3) to be exempt from the Investigational  
658 Device Exemption requirements in part 812 with the exception of 21 CFR section 812.119.  
659 If, however, you have concerns about the risk classification of your prospective clinical  
660 study, you should submit a risk-determination pre-submission as outlined in the “Requests  
661 for Feedback on Medical Device Submissions: The Pre-Submission Program and Meetings  
662 with Food and Drug Administration Staff”  
663 (<http://www.fda.gov/downloads/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/UCM311176.pdf>).  
664

665

666 Because patient numbers may be limited, you should consider a study design that collects  
667 multiple samples from patients over the course of their therapy. For example, consider  
668 designing studies to assess biodosimeter performance over the range of times post-exposure  
669 that you want to capture in labeling (such as 24 hours–7 days post-exposure). Samples  
670 should also be collected prior to radiation exposure whenever possible as control specimens.

671

672 We acknowledge that there are a number of challenges associated with prospectively  
673 collecting adequate clinical samples for device effectiveness testing. Therefore, it is  
674 recommended that you use the pre-submission process to discuss clinical study design and  
675 implementation prior to the onset of testing. Pre-submissions should ideally include the  
676 clinical validation study protocol, statistical analysis plan, and a description of sample  
677 acquisition strategies.

678

### **2. Retrospective clinical studies**

679

680

681 If the analyte or analytes being assessed by a biodosimetry device are suitably stable in the  
682 relevant test matrix, then you are encouraged to utilize appropriately banked retrospective  
683 samples to demonstrate the clinical performance of your biodosimetry device. For more  
684 information, please refer to the guidance entitled “Informed Consent for *In Vitro* Diagnostic  
685 Device Studies Using Leftover Human Specimens that are Not Individually Identifiable”  
686 (<http://www.fda.gov/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/ucm078384.htm>). Appropriate retrospective samples should have documentation on basic  
687 patient demographics (but not personally identifiable information) and basic information on  
688 the radiation exposure profile.  
689

690

### **3. Normal control samples**

691

692

693 Normal (unirradiated) control samples may be used both to assess the normal range of  
694 analyte expression and to create contrived samples by spiking the analyte of interest into an  
695 appropriate matrix. Assessment of the normal range of analyte expression should include a

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696 suitable number of normal control samples to determine if biodosimeter analyte expression is  
697 affected by subject age, race, gender, and common health conditions (e.g., obesity, diabetes,  
698 or arthritis). Normal control samples can be obtained prospectively or from appropriate  
699 sample banks. All normal control samples should be collected as intended for your device.  
700 For instance, if blood will be collected in EDTA tubes for use in your biodosimeter, then  
701 normal control samples should be collected in EDTA tubes. As above, basic demographic  
702 information and information on health conditions should be collected with normal control  
703 samples.

704

705

### **4. Limitations of clinical studies**

706

707 We acknowledge that there may be significant limitations in the interpretation of clinical  
708 studies for radiation biodosimetry submissions. For instance, therapeutic dose rates will not  
709 be reflective of the expected dose rates that would be experienced by someone in a  
710 radiological disaster. Additionally, clinical studies may not be reflective of all possible types  
711 of radiological disasters for which the biodosimeter is intended. Thus, in addition to the  
712 animal studies and analytical studies discussed above, biodosimetry submissions should  
713 include a discussion of the limitations of the clinical study, and how analytical studies,  
714 animal studies, or a combination of analytical and animal studies have been used to mitigate  
715 these limitations in order to demonstrate a reasonable assurance of the safety and  
716 effectiveness of the device for its intended use.

717

718

### **F. Labeling**

719

720 The labeling of a radiation biodosimetry device includes the instructions for use, package  
721 inserts, and any outer box or container labels for the device itself, reagents, and control  
722 materials, as applicable. The following references will be useful in developing clear and  
723 complete labeling for your device.

724

- 725 • The guidance entitled “Guidance on Medical Device Patient Labeling”  
726 (<http://www.fda.gov/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/ucm070782.htm>)
- 727 • CLSI document GP-14 “Labeling of Home-Use In Vitro Testing Products”
- 728 • Labeling Requirements – In Vitro Diagnostic Devices  
729 (<http://www.fda.gov/MedicalDevices/DeviceRegulationandGuidance/Overview/DeviceLabeling/InVitroDiagnosticDeviceLabelingRequirements/default.htm>)

730

731 In addition to the references above and the information already provided in this guidance  
732 document, the following should be considered when developing labeling for radiation  
733 biodosimetry devices that complies with the labeling requirements outlined in 21 CFR Parts  
734 801 and 809:

735

#### **1. Instructions for use**

736

737 For radiation biodosimeters intended for use by lay persons, information required by 21 CFR  
738 809.10(b) should be described in a manner that lay users can understand. Detailed technical

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739 information (e.g., scientific principles of test procedure or statistical analysis of data) may be  
740 presented in a separate section followed by clarifying statements appropriate for lay users.  
741 The following should also be taken into account when drafting appropriate instructions for  
742 use for radiation biodosimetry devices.

- 743 • The labeling must provide instructions for specimen collection and preparation (see  
744 21 CFR 809.10(b)(7)). Instructions should be drafted with the intended end user in  
745 mind. For example, consider whether a trained healthcare provider will be collecting  
746 the sample or if the patient will be instructed to do so.
- 747 • The labeling must provide a step-by-step outline of recommended procedures and  
748 operating instructions for the instrument (see 21 CFR 809.10(b)(8) and 21 CFR  
749 809.10(b)(6)(v)). Ideally, numbering rather than bullet points should be used for  
750 clarity.
- 751 • Labeling must describe details of calibration and of quality control procedures (see 21  
752 CFR 809.10(b)(8)(v) and 21 CFR 809.10(b)(8)(vi)). These instructions are to help  
753 ensure optimal performance of the system. This section should include  
754 recommendations for how and when to perform quality control checks and  
755 instructions for what to do if the control material values are not within the allowable  
756 ranges.

## 757 **2. Limitations**

758  
759 Labeling must include a statement of limitations of the procedure, including known extrinsic  
760 factors or interfering substances affecting results (see 21 CFR 809.10(b)(10)). You should  
761 also include testing conditions that may cause clinically significant errors due to bias or  
762 imprecision (e.g., combined injury, high dose rates, or alternative sources of radiation). You  
763 should also note all known contraindications. This section should thoroughly describe the  
764 situations of use that were not examined in performance testing of the device. For instance,  
765 if device performance was not assessed for performance using neutron radiation sources, then  
766 this information should be included in the labeling.

## 768 **3. Interpretation of results**

769  
770 Labeling must include expected values for your device (see 21 CFR 809.10(b)(11)). We  
771 recommend that the expected values be portrayed in terms of expected values for non-  
772 irradiated patients, and around the clinical decision making cut-points that were evaluated for  
773 your device (e.g., 2 Gy and 10 Gy). If the results are qualitative, you should explain how to  
774 interpret positive and negative results, including their clinical significance. If the results are  
775 quantitative, you should explain how numerical results correlate with expected values and the  
776 clinical significance of outputs. A statement should be included to interpret results in the  
777 context of other clinical signs and symptoms as well as any known dosimetric or radiation  
778 dispersal data associated with the patient's location.

779 You should also provide directions for the interpretation of the results of controls  
780 (performance monitors) and provide a statement that if controls do not perform as expected,

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781 assay results are invalid. Instructions should also be provided for any situation in which the  
782 end user should repeat a test.

### 783 **4. Performance characteristics**

784

785 Labeling must include specific performance characteristics of the device (see 21 CFR  
786 809.10(b)(12)). All studies, including bench testing, animal testing, and clinical studies  
787 should be summarized in the package insert of the assay. Performance data should be  
788 presented clearly and accurately, ideally in both graphical and text formats. Clinical  
789 information that was obtained through animal studies alone (with no human clinical  
790 supporting data) should be specifically highlighted with a disclaimer that the performance of  
791 the assay has not been evaluated in clinical samples under these specific conditions.

792

### 793 **G. CLIA Categorization**

794

795 As discussed above, some radiation biodosimeters may be designed for use in a clinical  
796 laboratory, while others may be designed to be used in a professional healthcare facility such  
797 as a hospital. Radiation biodosimeters intended to be used in initial triage may be designed  
798 to be performed outside of professional healthcare facilities or clinical laboratories by  
799 laypersons. The location where a device is intended to be used (e.g., clinical laboratory,  
800 professional healthcare facility, or home use) impacts the CLIA categorization of the device,  
801 and informs the kind of information that will need to be included in submissions to allow  
802 CLIA categorization to be completed. A document that may be of particular interest is the  
803 guidance entitled “Design Considerations for Devices Intended for Home Use”  
804 ([http://www.fda.gov/downloads/MedicalDevices/DeviceRegulationandGuidance/GuidanceD](http://www.fda.gov/downloads/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/UCM331681.pdf)  
805 [ocuments/UCM331681.pdf](http://www.fda.gov/downloads/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/UCM331681.pdf)). This guidance provides suggestions to assist manufacturers in  
806 designing and developing home use devices that comply with applicable standards of safety  
807 and effectiveness and other regulatory requirements.

808

809 CLIA (codified at 42 U.S.C. 263a) established uniform quality standards for all laboratory  
810 testing to ensure the accuracy, reliability and timeliness of patient test results throughout the  
811 United States. Under CLIA, laboratory tests are categorized according to complexity in  
812 order to determine what level of certification, if any, a laboratory or other user will be  
813 required to have in order to perform human diagnostic testing. As the complexity of a test  
814 increases, the number of entities certified to use it becomes more limited. Waived tests,  
815 which are simple tests, may be used by a variety of users, including inexperienced users.  
816 More complex tests known as moderate complexity tests may be performed in laboratories  
817 certified as moderate or high complexity (these can include health care provider offices).  
818 High complexity tests are those that are either difficult to perform or difficult to interpret, and  
819 may be performed by only specific clinical laboratories in the United States certified to  
820 perform high complexity testing.

821

822 Since 2000, CDRH has been responsible for categorizing commercially marketed IVDs  
823 under CLIA. CDRH determines the CLIA categorization of IVDs at the time of premarket  
824 submission. Thus, information pertaining to CLIA categorization should be included with



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825 the initial premarket submission. In particular, if your device is intended to be used in a field  
826 triage environment, you should design studies to demonstrate the performance of your  
827 device, including specific human factors, to verify performance by lay personnel in a non-  
828 laboratory setting. You are encouraged to review the guidance entitled “Administrative  
829 Procedures for CLIA Categorization”  
830 (<http://www.fda.gov/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/ucm070762.htm>)  
831 for information on how IVDs are categorized, and the information needed  
832 for CLIA waiver applications. In addition, the guidance entitled, “Design Considerations for  
833 Devices Intended for Home Use”  
834 (<http://www.fda.gov/downloads/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/UCM331681.pdf>)  
835 provides suggestions to assist manufacturers in designing and  
836 developing home use devices that comply with applicable standards of safety and  
837 effectiveness and other regulatory requirements.

838

## 839 **V. Appendix A: Statistical Considerations for Radiation** 840 **Biodosimetry Devices**

841

842 This appendix includes some statistical considerations for radiation biodosimetry devices.  
843 Further statistical considerations for diagnostic devices that may be applicable to radiation  
844 biodosimetry devices are comprehensively discussed in the guidance entitled “Statistical  
845 Guidance on Reporting Results from Studies Evaluating Diagnostic Tests”  
846 (<http://www.fda.gov/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/ucm071148.htm>)  
847 and further concepts and principles related to designing medical device  
848 studies are discussed in the guidance entitled “Design Considerations for Pivotal Clinical  
849 Investigations for Medical Devices”  
850 (<http://www.fda.gov/downloads/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/UCM373766.pdf>).  
851 In addition, as discussed above, it is recommended that you use  
852 the pre-submission process to discuss statistical analysis plans and methods before initiating  
853 any data collection for your clinical, pre-clinical and analytical studies.

854

### 855 **A. Independent Validation**

856

857 Validation of the performance of a radiation biodosimetry device should be conducted on  
858 subjects, which includes specimens from subjects that are independent of those used during  
859 device development. Before a validation study is conducted, all of the specifications for the  
860 assay (e.g., algorithm, probes, manufacturing methods, cut-off values) should be “locked  
861 down” (in the final version form). Generally, changes subsequent to validation would create  
862 the need for additional analytical and clinical validation studies separate from those already  
863 performed.

864

### 865 **B. Study Design**

866

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867 When evaluating the design of a study intended to establish the safety and effectiveness of a  
868 radiation biodosimetry device, a main consideration is whether the design could introduce  
869 non-negligible bias into the estimation of device performance. In a biased study design,  
870 estimates of device performance will tend to deviate systematically from the true  
871 performance of the device in the intended use population, regardless of the size of the study.  
872 For example, bias may be introduced in the selection of subjects, which includes specimens  
873 from subjects, study conduct, and mechanisms of data analysis, and may also arise from  
874 missing data. Understanding potential sources of bias and how to avoid or minimize them  
875 during the design of your study is essential. Some strategies for this purpose are described in  
876 the guidance entitled “Design Considerations for Pivotal Clinical Investigations for Medical  
877 Devices”  
878 (<http://www.fda.gov/downloads/MedicalDevices/DeviceRegulationandGuidance/GuidanceDocuments/UCM373766.pdf>). You may also refer to the extensive literature with  
879 comprehensive discussions on sources of bias in diagnostic devices studies.<sup>2</sup>  
880  
881

### **C. Study Integrity (Blinding)**

882  
883 To avoid bias in the device result, the user of the radiation biodosimetry device should be  
884 unaware of (i.e., blinded to) the actual level of radiation exposure (e.g., the administered dose  
885 or the level as measured by the clinical reference standard). Likewise, to avoid bias in the  
886 reference measurement, the user of the reference standard should be unaware of the device  
887 result. In general, the user should be unaware of any results from other diagnostic  
888 evaluations, and vice versa.  
889  
890

### **D. Precision of Estimation**

891  
892 The sampling variability or the precision of estimation is controlled by the sample size of the  
893 study and is another key consideration when evaluating a study design and study results.  
894 With a larger sample size, an estimate of performance is subject to less sampling variability.  
895 Uncertainty of the estimation is thus reduced. The estimate becomes less imprecise, leading  
896 to a narrower confidence interval of likely values for the true performance. If you have more  
897 than one study, the precision of estimation might be increased by a careful pre-planned  
898 analysis of combined studies, if appropriate.  
899  
900

### **E. Study Analysis**

901  
902 The protocol for a radiation biodosimeter study should include a Statistical Analysis Plan  
903 (SAP). The SAP is used to interpret the study data in support of the safety and effectiveness  
904 of the device for its intended use. The SAP should be pre-specified and provided in enough  
905 detail to permit FDA review. The analysis plan should define the performance measures  
906

---

<sup>2</sup> E.g., Pepe M, *The Statistical Evaluation of Medical Tests for Classification and Prediction*, Oxford, 2003; Zhou XH, Obuchowski NA, and McClish DK *Statistical Methods in Diagnostic Medicine*, 2<sup>nd</sup> ed, Wiley 2011; Begg C. Biases in the Assessment of Diagnostic Tests, *Stat Med* 1987; 6: 411-423.

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907 (e.g., specificity, sensitivity) to be evaluated. Any success criteria on the performance  
908 measures should be clearly pre-defined using descriptive and mathematical statements (e.g.,  
909 the null and alternative hypotheses for a significance test, the estimator for a performance  
910 measure, the method for deriving a confidence interval, etc.). Unplanned post-hoc analyses  
911 are discouraged as primary evidence of safety and effectiveness. Post-hoc analyses can  
912 inflate the study-wise type I error rate (probability of false statistical significance) and  
913 therefore are generally considered exploratory rather than confirmatory evidence of safety  
914 and effectiveness.

915

916 In particular, the SAP should describe how sample size for the study was determined.  
917 Sample size determination should be consistent with the pre-planned statistical analyses of  
918 the study, especially the primary analyses. Assumptions underlying the statistical power of  
919 the study to demonstrate a performance claim should be provided in detail.

920

921 The SAP should include a plan for dealing with device results that are considered  
922 uninterpretable, invalid, indeterminate, equivocal, or missing, and samples or specimens that  
923 are unavailable or unevaluable. For example, the plan may include reporting the number and  
924 proportion of subjects without a valid device result by the reason a valid result was not  
925 obtained. If repeated application (after the first reading) of the device on a subject or  
926 specimen is not intended, is not possible, or would not be helpful (e.g., the device result will  
927 always be uninterpretable), then uninterpretable device results, for example, could be treated  
928 as a separate category for the purpose of analysis. If repeat measurement of subjects or  
929 specimens is possible and appropriate, then imputation of missing device results can  
930 sometimes aid the statistical analysis and interpretation of study data. Further comments  
931 with respect to missing data are in section V(E)(4) below.

932

933 If the design of your study is adaptive, its adaptive features should be pre-planned (i.e., the  
934 study should be adaptive *by design*). Before conducting an adaptively designed study, its  
935 operating characteristics (e.g., type 1 error rate, power) and its potential for introducing  
936 operational bias into the study (due to the adaptive features) should be evaluated. Some  
937 examples of adaptations based on interim analysis include stopping the study early for futility  
938 or success, re-estimating sample size, and changing a hypothesis. Monitoring a study until it  
939 has a pre-defined number of subjects with or without a condition is an adaptive design  
940 feature which does not ordinarily require special consideration. The literature on adaptive  
941 design for diagnostic studies is unfortunately scant, but some references are available.<sup>3</sup>

942

### 943 **1. Quantitative, continuous, or semi-quantitative output**

944

945 Statistical analyses and methods depend on the type of results provided by the radiation  
946 biodosimetry device. For devices providing a quantitative measurement, the bias and

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<sup>3</sup> Gerke O, Hoiland-Carlsen PF, Poulsen MH, Vach W. Interim analyses in diagnostic versus treatment studies: Differences and similarities. *Am J Nucl Med Mol Imaging* 2012; 2(3): 344–52; Tang LL, and Liu A. Sample size recalculation in sequential diagnostic trials, *Biostatistics* 2010; 11(1): 151-163.



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947 imprecision of the measurement should be evaluated along with other performance  
948 characteristics. For example, Bland-Altman methodology can be used to compare the level  
949 of radiation exposure predicted by the device with the actual level of exposure (actual dose or  
950 reference level) over the measuring interval.<sup>4</sup> Comparison of device and reference results  
951 near clinical decision making cut-points is essential. The bias of the device result should be  
952 estimated near these decision points. Please refer to the CLSI document EP09-A3,  
953 “Measurement Procedure Comparison and Bias Estimation Using Patient Samples; Approved  
954 Guideline-Third Edition,” and EP5-A2, “Evaluating of Precision Performance of  
955 Quantitative Methods; Approved Guideline-Second Edition.”

956  
957 Receiver Operating Characteristic (ROC) analysis might also be useful to evaluate the  
958 diagnostic accuracy of a radiation biodosimetry device reporting a quantitative, continuous,  
959 or semi-quantitative result, or reporting a qualitative result derived from an underlying value  
960 that is quantitative, continuous, or semi-quantitative. ROC analysis evaluates the overall  
961 ability of the device to discriminate between subjects with and without a condition of  
962 interest. On an ROC plot, the false positive and true positive fractions (1 – specificity,  
963 sensitivity) are plotted for each possible cut-off in the value as it is varied across the entire  
964 range of observed values, resulting in an ROC “curve.” An advantage of ROC analysis can  
965 be that the plot will display the estimated sensitivity and specificity of the device throughout  
966 a range of clinical decision making points. The area under the ROC curve (AUC) is a global  
967 measure of device discrimination performance, with AUC values of 0.5 and 1.0 indicating  
968 random and perfect discrimination, respectively. Please refer to the CLSI document EP24-  
969 A2, “Assessment of the Diagnostic Accuracy of Laboratory Tests Using Receiver Operating  
970 Characteristic Curves; Approved Guideline-Second Edition,” as well as the following  
971 references.<sup>5</sup> If the condition of interest is not binary (e.g., dose or level of radiation  
972 exposure), generalizations of AUC exist for evaluating the discrimination ability of medical  
973 tests.<sup>6</sup>

## **2. Qualitative output**

974  
975  
976  
977 For devices that are designed to provide a qualitative output around a clinical decision  
978 making cut-point, device evaluation should include its performance metrics using measures  
979 such as sensitivity, specificity, and the negative and positive diagnostic likelihood ratios  
980 (NLR, PLR). PLR is defined as sensitivity / (1 – specificity), the ratio of the true positive

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<sup>4</sup> Bland JM, Altman DG. Measuring agreement in method comparison studies. *Statistical Methods in Medical Research* 1999; 8 (2): 135–60.

<sup>5</sup> Pepe M, *The Statistical Evaluation of Medical Tests for Classification and Prediction*, Oxford, 2003; Zhou XH, Obuchowski NA, and McClish DK, *Statistical Methods in Diagnostic Medicine Bias*, 2<sup>nd</sup> ed, Wiley, 2011; Zou K, *Statistical Evaluation of Diagnostic Performance – Topics in ROC Analysis*, Chapman & Hall/CRC, 2012; Krzanowski WJ, and Hand DJ. *ROC Curves for Continuous Data*, Chapman & Hall/CRC, 2009; Zweig MH, and Campbell G. Receiver-Operating Characteristic (ROC) Plots: A Fundamental Evaluation Tool in Clinical Medicine, *Clin Chem* 1993; 39(4): 561-577.

<sup>6</sup> Obuchowski NA. An ROC-type measure of diagnostic accuracy when the gold standard is continuous-scale. *Stat Med* 2006; 25: 481-493; Obuchowski NA. Estimating and comparing diagnostic tests' accuracy when the gold standard is not binary, *Acad Radiol* 2005; 12:1198–1204.

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981 fraction to the false positive fraction. NLR is defined as  $(1 - \text{sensitivity}) / \text{specificity}$ , the  
982 ratio of the false negative fraction to the true negative fraction. Larger values of PLR and  
983 smaller values of NLR indicate better classification of the condition status. PLR and NLR  
984 are proportional to the odds that test positive and negative subjects have a condition,  
985 respectively.

986

987 Corresponding two-sided 95% confidence intervals should be provided. The method used to  
988 estimate these measures and their corresponding 95% confidence intervals should be clearly  
989 pre-specified. If multiple measurements are obtained per subject, the statistical analysis (e.g.,  
990 95% confidence interval) should account for the correlation structure of the within-subject  
991 measurements using a valid statistical method.

992

993

### 3. Analytical imprecision for qualitative devices

994

995 Imprecision is a quantitative value that indicates the extent of disagreement or variability of a  
996 set of replicate measurements. For radiation biodosimetry devices providing a quantitative or  
997 continuous value (e.g., radiation dose or level), the standard deviation and coefficient of  
998 variation are common measures of imprecision. Repeatability is the imprecision when  
999 repeated measurements are taken under the same conditions of measurement. Intermediate  
1000 imprecision is the imprecision when the repeated measurements are taken with some  
1001 conditions intentionally varied (e.g., run, day, operator, instrument, reagent lot). See CLSI  
1002 document EP05-A3, “Evaluation of Precision of Quantitative Measurement Procedures—  
1003 Third Edition.”

1004

1005 For biodosimetry devices intended to report qualitative results, the percent agreement of the  
1006 replicate device results with the qualitative result that is expected for the subject or specimen  
1007 may be reported. Alternatively, a pure measure of imprecision analogous to the standard  
1008 deviation for continuous replicate results is the Gini index (or Gini variability). The Gini  
1009 index is the probability that two categorical results in replicate testing (for the same sample)  
1010 fall into different categories. For  $J$  categories,  $g = 1 - \sum_{j=1}^J p_j^2$ , where  $p$  denotes the  
1011 probability that a replicate gives a result from category  $J$ . For two categories,  $g = 1 - p^2 - (1-p)^2$   
1012  $= 2p(1-p) = 2\text{Var}(X)$  for Bernoulli random variable  $X$  that takes values 1 and 0 with  
1013 probabilities  $p$  and  $1 - p$ . Further details on the Gini index are available in literature  
1014 references.<sup>7</sup>

1015

1016

### 4. Missing data

1017

1018 The SAP should describe how missing data will be handled and documented. Reported  
1019 results can be misleading if subjects with missing measurement results are excluded from the

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<sup>7</sup> Agresti (2002), *Categorical Data Analysis*, 2<sup>nd</sup> Ed., p. 68, Light and Margolin (1971), *An Analysis of Variance for Categorical Data*, *Journal of the American Statistical Association*, 66 (335), pp. 534-544, Bishop, Fienberg and Holland (1975), *Discrete Multivariate Analysis: Theory and Practice*, MIT Press, Cambridge, MA. Light RJ, and Margolin BH, *An analysis of variance for categorical data*, *J Amer Stat Assoc* 1971; 66(335): 534-544.

1020 analysis, the report, or both the analysis and the report. All subjects for whom a  
1021 measurement was attempted need to be accounted for when reporting results. It is important  
1022 to analyze the impact of missing data on the conclusions obtained from the study. In some  
1023 cases it may be necessary to assess if study conclusions are robust given the missing data,  
1024 and in such cases an intent-to-diagnose or ITD analysis can be performed. An ITD analysis  
1025 includes every subject or specimen, regardless of whether the subject or specimen is missing  
1026 the radiation biodosimetry device result, the actual dose, the clinical reference diagnosis, or  
1027 other results from comparators.  
1028

## 1029 **F. Feature Selection During Algorithm Development**

1030  
1031 If your radiation biodosimetry device incorporates multiple pieces of information into an  
1032 algorithm in order to produce a single output, validation of this algorithm will be important to  
1033 understand the performance capabilities of the assay. During algorithm development, it is  
1034 generally important to obtain a trustworthy estimate of the algorithm's performance before  
1035 the pivotal performance validation study. Cross-validation is a procedure for estimating the  
1036 performance of an algorithm on the same dataset on which it was developed. The  
1037 developmental dataset is split repeatedly into training and test datasets, with the algorithm  
1038 developed on the training set and evaluated on the test set. The performance estimates  
1039 obtained for the many splits are then averaged. In bootstrap cross-validation, a training set of  
1040 the same size as the original dataset is obtained by sampling the subjects or specimens with  
1041 replacement and evaluated on the remaining unselected subjects or specimens.<sup>8</sup> Cross-  
1042 validation requires that algorithm development be automated, so may not be possible if the  
1043 algorithm development process has subjective aspects. All steps of the algorithm  
1044 construction process, including and especially the step of selecting the features (analytes,  
1045 measurands, etc.) to be used by the algorithm, should be cross-validated, otherwise the  
1046 performance estimate will likely be biased.<sup>9</sup> Please note that internal cross-validation is not a  
1047 substitute for pivotal validation in a dataset that is independent of (external to) the datasets  
1048 used for development. Further, for the pivotal validation, the final version of the test should  
1049 be used.  
1050

## 1051 **G. Electronic Data**

1052  
1053 You are encouraged to provide an electronic version of the line data with your submission in  
1054 an appropriate format such that the datasets are well-described and interpretable. These and  
1055 the associated programs used to generate your results should be included in a format which  
1056 can be easily transferred into statistical software. The information at the following URL may  
1057 be helpful as you prepare these materials:  
1058

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<sup>8</sup> Efron B, and Tibshirani R. Improvements on Cross-Validation: The .632+ Bootstrap Method. *J Amer Statist Assoc* 1997; 92(438): 548-560.

<sup>9</sup> Simon R et al, Pitfalls in the Use of DNA Microarray Data for Diagnostic and Prognostic Classification, *J National Cancer Institute* 2003; 95(1):14-18.

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1059 [http://www.fda.gov/MedicalDevices/DeviceRegulationandGuidance/HowtoMarketYourDevi](http://www.fda.gov/MedicalDevices/DeviceRegulationandGuidance/HowtoMarketYourDevice/PremarketSubmissions/ucm136377.htm)  
1060 [ce/PremarketSubmissions/ucm136377.htm](http://www.fda.gov/MedicalDevices/DeviceRegulationandGuidance/HowtoMarketYourDevice/PremarketSubmissions/ucm136377.htm)

1061

## 1062 **VI. Appendix B: References**

1063

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